Debiasing incorporated into reconstruction of low-rank modelled dynamic MRI data

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Joint debiasing

Perfusion DCE-MRI reconstruction L

 $\arg\min\frac{1}{2}\|\mathbf{Y} - E(\mathbf{L})\|_{\mathrm{F}}^{2} + \lambda\|\mathbf{L}\|_{*}$

- Y is the matricized k-t-space data
- E is the respective subsampled Fourier transform
- Computed using proximal gradient algorithm
- After each iteration, SVD of $\mathbf{L}^{(k)}$ is known:

 $\mathbf{L}^{(k)} = \mathbf{U}^{(k)} \cdot \operatorname{diag}(\sigma_1^{(k)}, \sigma_2^{(k)}, \dots, \sigma_r^{(k)}) \cdot \mathbf{V}^{(k)*}$

Debiasing

$\arg\min_{\sigma_1,\sigma_2,\ldots,\sigma_r>0} \left\| \mathbf{Y} - E(\mathbf{U}_r^{(k)} \cdot \operatorname{diag}(\sigma_1,\sigma_2,\ldots,\sigma_r) \cdot \mathbf{V}_r^{(k)*}) \right\|_{\mathrm{F}}^2$ (2) $\sigma_i \in \mathbb{R}$

problem (compressed

sensing, CS)

Biased

15 20 perfusion

curves

(1)

It gives biased estimates



1.8

1.6

- using Matlab
- Phantom of 100 × 100 px × 100 time points in size
- Perturbed by additive Gaussian noise with standard deviation 0.05

Method

Solved by repeating several times: gradient step w.r.t.

 σ_i and projecting result to real, non-negative values



- Used 100 radials per frame with random slopes of spokes
- Using (1) with postdebiasing (2) led to worse reconstruction than joint debiasing algorithm



Realdata Free-breathing abdominal DCE-MRI

data [3]

- The acquisition used golden-angle
 - scheme with a 12-element receiver

coil array

21 golden-angle radial trajectories per

frame were used

With joint debiasing, perfusion curves



enjoy higher initial peak and the

second peak is more readable



With joint debiasing

References

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[2] Ma, S.: Algorithms for Sparse and Low-Rank Optimization: Convergence, Complexity and Applications, Disertation thesis, Columbia University, 2011.

[3] Otazo, R., Candes, E., Sodickson, D.K. Low-rank plus sparse matrix decomposition for accelerated dynamic MRI with separation of background and dynamic components. Magnetic Resonance in Medicine, 73(3), 2015.